Multiphysics in Haemodynamics: Fluid-Structure Interaction between Blood and Arterial Wall

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Joint work with: L. Formaggia, A. Moura, C. Vergara, MOX

Acknowledgements: P. Causin, J.F. Gerbeau

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Outline

Introduction

- 2 Mathematical problem
 - Governing equations
 - Global weak formulation
 - Energy inequality

8 Numerical approximation and stability analysis

- ALE framework
- Partitioned algorithms
- Added mass effect

Absorbing boundary conditions

- 1D hyperbolic model
- Absorbing boundary conditions

5 Numerical results

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Introduction

Mathematical problem Numerical approximation and stability analysis Absorbing boundary conditions Numerical results

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Introduction

Local fluid dynamics is related to the development of vascular diseases



Peculiarities

- Pulsatile flow (heart beat $\sim 1 sec$)
- Relatively large displacements
 - ⇒ fluid domain movement non negligible
- Wave propagation due to fluid structure interaction

$$\implies$$
 characteristic time: $t = \frac{L}{v} \approx \frac{0.25m}{5m/s} = 0.05sec$



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Governing equations Global weak formulation Energy inequality

Physical Model



- Fluid equations defined in the moving domain Ω^f_t . Typically written in Eulerian form
- Structure equations typically written in Lagrangian form on the reference domain Ω_0^s .

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Physical Model – Fluid

•Blood can be treated as a homogeneous, incompressible, Newtonian fluid in large arteries.

Navier-Stokes equations

$$\begin{cases} \varrho_f \frac{\partial \mathbf{u}}{\partial t} + \varrho_f \operatorname{div}(\mathbf{u} \otimes \mathbf{u}) - \operatorname{div} \boldsymbol{\sigma}_f(\mathbf{u}, p) = \mathbf{f}^f \\ \operatorname{div} \mathbf{u} = 0 \\ + \text{ suitable initial and boundary conditions} \end{cases}$$

- u: fluid velocity $D(u) = \frac{\nabla u + \nabla^T u}{2}$: strain tensor
- p: fluid pressure

 $\sigma_{f}(\mathbf{u}, p) = 2\mu \mathbf{D}(\mathbf{u}) - p\mathbf{I}$: fluid stress tensor

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Physical Model – Structure

- Arteries are (relatively) thin, multilayered structures, which deform principally in the radial direction.
- Deformations can reach up to 10% of the artery diameter
- Several models have been proposed: 3D non-linear elasticity, shell (membrane) models, simplified models only for radial displacement.

Non-linear elasticity

Unknown: Structure displacement $\eta(t,\xi) = \mathbf{x}(t,\xi) - \xi$



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$$arrho_s^0 rac{\partial^2 oldsymbol{\eta}}{\partial t^2} - \mathsf{div}_0 \left[\mathbf{F}(oldsymbol{\eta}) \mathbf{S}(oldsymbol{\eta})
ight] = f_0^s, \quad ext{in } \Omega_0^s,$$

where $\mathbf{F} = \mathbf{I} + \nabla_0 \boldsymbol{\eta}$: deformation gradient

 $J(\eta) = \det(F(\eta))$: change of volume

$$\mathbf{E} = \frac{1}{2} (\mathbf{F}^T \mathbf{F} - \mathbf{I})$$
: Green strain tensor

 \mathbf{S} : second Piola-Kirchhoff stress tensor

Constitutive law

Hyperelastic materials

St. Venant-Kirchhoff materials

 $\mathbf{S} = \frac{\partial W(\mathbf{E})}{\partial \mathbf{E}}, \qquad (W: \text{ elastic energy})$ $\mathbf{S} = \lambda \operatorname{tr}(\mathbf{E})\mathbf{I} + 2\mu \mathbf{E}$

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Physical Model – Coupling conditions

On reference interface Γ_0

•Continuity of velocity (kinematic condition)

$$\mathbf{u} \circ \mathbf{x}(\boldsymbol{\xi}) = \frac{\partial \boldsymbol{\eta}}{\partial t}$$

•Continuity of normal stress (dynamic condition)

$$J(\boldsymbol{\eta})\boldsymbol{\sigma}_f(\mathbf{u},\boldsymbol{\rho})\boldsymbol{F}^{-T}(\boldsymbol{\eta})\mathbf{n}_0^f = -\boldsymbol{F}(\boldsymbol{\eta})\boldsymbol{S}(\boldsymbol{\eta})\mathbf{n}_0^s$$

with $\mathbf{n}_0^f = -\mathbf{n}_0^s$.

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A global weak formulation

Fluid eqs. Multiply by $(v, q) \in \mathbf{H}^{1}_{\Gamma_{D}}(\Omega^{f}_{t}) \times L^{2}(\Omega^{f}_{t})$

$$\int_{\Omega_t^f} \varrho_f \left(\frac{\partial \mathbf{u}}{\partial t} + \operatorname{div}(\mathbf{u} \otimes \mathbf{u}) \right) \cdot \mathbf{v} + \boldsymbol{\sigma}_f : \nabla \mathbf{v} + \operatorname{div} \mathbf{u} q = \int_{\Omega_t^f} \mathbf{f} \cdot \mathbf{v} + \int_{\Gamma_t} (\boldsymbol{\sigma}_f \cdot \mathbf{n}^f) \cdot \mathbf{v}$$

Structure eq. Multiply by $\phi \in \mathbf{H}^{1}_{\Gamma_{D}}(\Omega_{0}^{s})$

$$\int_{\Omega_0^s} \varrho_s^0 \frac{\partial^2 \boldsymbol{\eta}}{\partial t^2} \cdot \boldsymbol{\phi} + \mathbf{F}(\boldsymbol{\eta}) \mathbf{S}(\boldsymbol{\eta}) : \nabla_0 \boldsymbol{\phi} = \int_{\Omega_0^s} f_0^s \cdot \boldsymbol{\phi} + \int_{\Gamma_0} (\mathbf{F}(\boldsymbol{\eta}) \mathbf{S}(\boldsymbol{\eta}) \cdot \mathbf{n}_0^s) \cdot \boldsymbol{\phi}$$



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Global weak formulation - cont.

•If we take matching test functions at the interface: $\mathbf{v} \circ \mathbf{x}(\boldsymbol{\xi}) = \phi(\boldsymbol{\xi})$ and thanks to the coupling condition (continuity of stresses), the interface terms perfectly cancel.

Fluid-Structure functional space

$$V \equiv \{(\mathbf{v}, q, \phi): \ \mathbf{v} \circ \mathbf{x}(\boldsymbol{\xi}) = \phi(\boldsymbol{\xi}) \ \text{ on } \Gamma_0\}$$

$$\int_{\Omega_t^f} \varrho_f \left(\frac{\partial \mathbf{u}}{\partial t} + \operatorname{div}(\mathbf{u} \otimes \mathbf{u}) \right) \cdot \mathbf{v} + \boldsymbol{\sigma}_f(\mathbf{u}, \boldsymbol{\rho}) : \nabla \mathbf{v} + \operatorname{div} \mathbf{u} q + \int_{\Omega_0^s} \varrho_s^0 \frac{\partial^2 \boldsymbol{\eta}}{\partial t^2} \cdot \boldsymbol{\phi} + \mathbf{F}(\boldsymbol{\eta}) \mathbf{S}(\boldsymbol{\eta}) : \nabla_0 \boldsymbol{\phi} = \int_{\Omega_t^f} \mathbf{f}^f \cdot \mathbf{v} + \int_{\Omega_0^s} f_0^s \cdot \boldsymbol{\phi}$$

+ coupling condition $\mathbf{u} \circ \mathbf{x}(\boldsymbol{\xi}) = \frac{\partial \eta}{\partial t}$



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Energy inequality

•Taking as test functions $(\mathbf{v},q,\phi)=(\mathbf{u},p,\dot{\eta})$ we can derive an Energy inequality

Fluid Structure Energy (kinetic + elastic)

$$\mathcal{E}(t) \equiv rac{arrho_f}{2} \|\mathbf{u}(t)\|_{L^2(\Omega_t^f)}^2 + rac{arrho_0^5}{2} \|rac{\partial \eta}{\partial t}(t)\|_{L^2(\Omega_0^5)}^2 + \int_{\Omega_t^5} W(\eta)(t)$$

Then (homogeneous problem)

$$\mathcal{E}_{FS}(T) + 2\mu \int_0^T \int_{\Omega_t^f} \mathbf{D}(\mathbf{u}) : \mathbf{D}(\mathbf{u}) \, d\Omega \, dt \leq \mathcal{E}_{FS}(0)$$

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Energy Inequality

Key points in deriving an energy inequality:

• Perfect balance of work at the interface

$$\int_{\Gamma_t} (\boldsymbol{\sigma}_f \cdot \mathbf{n}^f) \cdot \mathbf{u} = - \int_{\Gamma_0} (\mathbf{F}(\boldsymbol{\eta}) \mathbf{S}(\boldsymbol{\eta}) \cdot \mathbf{n}_0^s) \cdot \frac{\partial \boldsymbol{\eta}}{\partial t}$$

• No kinetic flux through the interface

(time der.)
$$\int_{\Omega_t^f} \varrho_f \frac{\partial \mathbf{u}}{\partial t} \cdot \mathbf{u} = \frac{\varrho_f}{2} \frac{d}{dt} \int_{\Omega_t^f} |\mathbf{u}|^2 - \frac{\varrho_f}{2} \int_{\Gamma_t} |\mathbf{u}^2| \mathbf{w} \cdot \mathbf{n}$$

(convective term)
$$\int_{\Omega_t^f} \varrho_f \operatorname{div}(\mathbf{u} \otimes \mathbf{u}) \cdot \mathbf{u} = \frac{\varrho_f}{2} \int_{\Gamma_t} |\mathbf{u}^2| \mathbf{u} \cdot \mathbf{n}$$

where **w** is the velocity at which the interface moves. Since $\mathbf{w} = \mathbf{u} = \dot{\eta}$, the kinetic flux $\frac{\varrho_f}{2} \int_{\Gamma_f} |\mathbf{u}^2| (\mathbf{u} - \mathbf{w}) \cdot \mathbf{n}$ vanishes.

• This does not hold if one couples Stokes with a non-linear structure

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Other structure models

• Assuming a cylindrical reference configuration, simpler models have been proposed, accounting only for radial displacement $\eta : \Gamma_0 \to \mathbb{R}$. They reproduce correctly the pressure wave propagation.

Independent ring:
$$\varrho_0^s h_s \frac{\partial^2 \eta}{\partial t^2} + \frac{Eh_s}{(1-\nu^2)R_0^2} \eta = f_s$$

Algebraic law:

$$\frac{Eh_s}{(1-\nu^2)R_0^2}\eta=f_s$$

Coupling conditions: $\mathbf{u} \circ \mathbf{x}(\boldsymbol{\xi}) = \frac{\partial \eta}{\partial t} \mathbf{e}_r$, $f_s = \mathbf{e}_r^T \left[J \sigma_{\mathbf{f}}(\mathbf{u}, p) F_t^{-T} \right] \mathbf{e}_r$

- Global weak formulations and energy inequalities can be derived in these cases as well
- Well posedness. Only partial results available even for 2D problems and simple structure models. (Y. Maday, C. Grandmont, B. Desjardens, M, Esteban, H. Beirao da Veiga, D. Coutand, ...)

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Numerical Approximation

•Space discretization by Finite Elements both for the fluid and the structure.

Major difficulties

- Discretize fluid equations on a moving domain ⇒ ALE formulation
- Find stable time discretization schemes and coupling strategies.



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ALE framework Partitioned algorithms Added mass effect

ALE Formulation

•The moving domain is recast at each time t to a fixed configuration Ω_0^f through the ALE mapping \mathcal{A}_t :



 $egin{aligned} &\mathcal{A}_t: \Omega_0 \longrightarrow \Omega_t, \ &\mathbf{x}(\boldsymbol{\xi},t) = \mathcal{A}_t(\boldsymbol{\xi}) \end{aligned}$



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domain velocity

ALE derivative

$$\begin{split} \mathbf{w}(\mathbf{x},t) &= \frac{\partial \mathcal{A}_t}{\partial t} \circ \mathcal{A}_t^{-1}(\mathbf{x}) \\ \left. \frac{\partial \mathbf{u}}{\partial t} \right|_{\boldsymbol{\xi}} &= \left. \frac{\partial \mathbf{u}}{\partial t} \right|_{\mathbf{x}} + \mathbf{w} \cdot \nabla_{\mathbf{x}} \mathbf{u} \end{split}$$



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Navier-Stokes ALE

$$\begin{cases} \varrho_f \frac{\partial \mathbf{u}}{\partial t} \Big|_{\boldsymbol{\xi}} + \varrho_f (\mathbf{u} - \mathbf{w} \cdot \nabla) \mathbf{u} - \operatorname{div} \boldsymbol{\sigma}_f (\mathbf{u}, \boldsymbol{p}) = \mathbf{0} \\ \operatorname{div} \mathbf{u} = \mathbf{0} \end{cases} \quad \text{in } \Omega_t \end{cases}$$

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Finite Element ALE approximation

- We introduce a mesh T_{h0} in the reference domain. The ALE mapping induces a mesh T_{ht} in Ω_t at each time t.
- Given the deformation of the boundary, the ALE mapping can be built by interpolation or solution of a differential problem (e.g. harmonic extension of the boundary displacement)
- The unknowns are associated to the nodes of \mathcal{T}_{ht} , which move in time.
- The ALE derivative is the derivative of the unknowns along the trajectories of the nodes; it can be easily discretized
- The discretization of the spatial operators is done on the current configuration Ω_t (much easier).



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Partitioned algorithms

•The fluid-structure coupled system is highly non linear since the fluid domain Ω_t^f , the ALE mapping \mathcal{A}_t and the domain velocity **w** all depend on the unknown displacement η . A direct solution of the global non-linear system (monolithic approach) is very costly.

•Partitioned time marching algorithms are based on subsequent solutions of fluid and structure subproblems

- allow one to reuse existing computational codes.
- each subproblem can be solved with the most efficient available numerical algorithms (e.g. projection schemes for Navier-Stokes, updated Lagrangian for structure dynamics,)

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ALE framework Partitioned algorithms Added mass effect

Explicit partitioned algorithms also called "loosely coupled" or "staggered"

In each time step solve only once (or just a few times) the fluid and structure problems

Example

- 1. Solve structure pb. with Neumann b.cs $(\eta^n = \eta^n(\sigma_f(\mathbf{u}^{n-1}, p^{n-1})))$
- 2. Update fluid mesh $(A_{t^n} = A_{t^n}(\eta^n))$
- 3. Solve fluid pb. with Dirichelet b.cs (compute (\mathbf{u}^n, p^n))
- 4. go to next time step
 - Typically obtained by combining an explicit discretization for the structure and an implicit discr. for the fluid.
 - The continuity of the stresses at the interface is not satisfied exactly.
 ⇒ Energy is not perfectly balanced.
 - A predictor corrector strategy can be added to the algorithm [see C. Farhat, S. Piperno, ...] to reduce the "energy error"



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Implicit partitioned algorithms

$\bullet At$ each time step enforce exactly both coupling conditions at the interface (Energy balanced)

•All the equations are coupled in each time step \implies need subiterations

Example: Fixed point (or Dirichlet Neumann) iterations

In each time step $[t^n, t^{n+1}]$, and $\forall k > 0$ solve

- 1. Solve structure pb. with Neumann b.cs $(\eta_k = \eta_k(\sigma_f(\mathbf{u}_{k-1}, p_{k-1})))$
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- 4. Recompute structure $(\eta_{k+1} = \eta_{k+1}(\sigma_f(u_k, p_k)))$
- 5. if $\|\eta_{k+1} \eta_k\| < tol$ then go to next time step else relax the solution η_{k+1} and go to 2.

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Numerical observations

In haemodymanics applications (thin structure in cylindrical configuration) **numerical tests** [Nobile, Ph.D] show that explicit algorithms become unstable when

- $\varrho_s^0 h_s / \varrho_f$ small
- L/D large (L=length, D=diameter of the tube)

irrespectively of the time step chosen!!!

•Under the same conditions, implicit Block Gauss-Seidel iterative algorithms need very small relaxation parameters to converge.

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How to get stable implicit schemes: example IE+BDF

•Let us start from the global weak (ALE) formulation and consider as time discretization: Implicit Euler (fluid) and BDF1 (structure)

$$\begin{split} \varrho_f \frac{d}{dt} \int_{\Omega^f(t)} \left(\mathbf{u} + \operatorname{div}(\mathbf{u} \otimes (\mathbf{u} - \mathbf{w})) \right) \cdot \mathbf{v} + \sigma_f(\mathbf{u}, p) : \nabla \mathbf{v} + \operatorname{div} \mathbf{u} q + \\ \int_{\Omega_0^s} \varrho_s^0 \frac{\partial^2 \eta}{\partial t^2} \cdot \phi + \mathbf{F}(\eta) \mathbf{S}(\eta) : \nabla_0 \phi = \int_{\Omega_t^f} \mathbf{f}^f \cdot \mathbf{v} + \int_{\Omega_0^s} f_0^s \cdot \phi \end{split}$$

+ coupling condition $\mathbf{u}^n \circ \mathbf{x}(\boldsymbol{\xi}) = \frac{\partial \boldsymbol{\eta}}{\partial t}$



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$$\frac{\varrho_f}{\Delta t} \int_{\Omega^f(t^n)} \mathbf{u}^n \cdot \mathbf{v} - \frac{\varrho_f}{\Delta t} \int_{\Omega^f(t^{n-1})} \mathbf{u}^{n-1} \cdot \mathbf{v} + \int_{\Omega^f(t^n)} \varrho_f \operatorname{div}(\mathbf{u}^n \otimes (\mathbf{u}^n - \mathbf{w}^n)) \cdot \mathbf{v} + \int_{\Omega^f(t^n)} \sigma_f(\mathbf{u}^n, p^n) : \nabla \mathbf{v} + \operatorname{div} \mathbf{u}^n q + \int_{\Omega_0^s} \varrho_s^0 \frac{\eta^n - 2\eta^{n-1} + \eta^{n-2}}{\Delta t^2} \cdot \phi + \mathbf{F}(\eta^n) \mathbf{S}(\eta^n) : \nabla_0 \phi = \int_{\Omega^f(t^n)} \mathbf{f}^f(t^n) \cdot \mathbf{v} + \int_{\Omega_0^s} f_0^s(t^n) \cdot \phi$$

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How to get stable implicit schemes: example IE+BDF

 To get global stability, the ALE-convective term has to be integrated on intermediate configurations so as to satisfy the so called Geometric Conservation Laws (GCL) [Formaggia-Nobile, '99, '04]

Stability Result for homogeneous problem [Nobile, PhD]

$$\begin{split} \frac{\varrho_f}{2} \|\mathbf{u}^n\|_{L^2(\Omega^f(t^n))}^2 &+ \frac{\varrho_0^s}{2} \|\frac{\boldsymbol{\eta}^n - \boldsymbol{\eta}^{n-1}}{\Delta t}\|_{L^2(\Omega_0^s)}^2 + \int_{\Omega_0^s} W(\boldsymbol{\eta}^n) \, d\Omega \\ &+ \sum_i \Delta t \int_{\Omega^f(t^i)} \mathbf{D}(\mathbf{u}^i) : \mathbf{D}(\mathbf{u}^i) \, d\Omega \\ &\leq \frac{\varrho_f}{2} \|\mathbf{u}^0\|_{L^2(\Omega_0^f)}^2 + \frac{\varrho_0^s}{2} \|\dot{\boldsymbol{\eta}}^0\|_{L^2(\Omega_0^s)}^2 + \int_{\Omega_0^s} W(0) \, d\Omega \end{split}$$

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Mathematical explanation of instabilities

We consider an over-simplified model:

- Fluid model: potential flow (no viscous and convective terms; only the incompressibility of the fluid is kept)
- Fluid geometry is kept fixed
- Independent rings model for the structure

•This model features the same numerical instabilities as the more complex (and non-linear) one.

Conclusions: the source of the instability is the *incompressibility of the fluid*

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Simple FSI model



 $\label{eq:structure} \begin{array}{c} \rho_{w}h_{s}\partial_{tt}^{2}\eta-a\partial_{xx}^{2}\eta+b\eta=\textbf{\textit{p}} \quad \text{on } \boldsymbol{\Sigma} \end{array}$

Fluid
$$\begin{cases} \rho_f \partial_t \mathbf{u} + \nabla p = 0 & \text{on } \Omega_F \\ \operatorname{div} \mathbf{u} = 0 & \xrightarrow{\operatorname{div}} \\ \mathbf{u} \cdot \mathbf{n} = \partial_t \eta & \text{on } \Sigma \\ + b.c. & \xrightarrow{\operatorname{div}} \end{cases} \quad \begin{cases} \Delta p = 0 \\ \partial_n p = -\rho_f \partial_{tt}^2 \eta \\ + b.c. \end{cases}$$

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Functional setting

For any $w \in H^{-1/2}(\Sigma)$, we denote by $\mathcal{R}w$ solution to the following problem

$$\begin{cases} -\Delta \mathcal{R} w = 0 & \text{in } \Omega_F, \\ \frac{\partial \mathcal{R} w}{\partial n} = w & \text{on } \Sigma \\ + \text{ homogeneous b.c.} & \text{on } \Gamma_F^1, \Gamma_F^2, \Gamma_F^3 \end{cases}$$

Added mass operator: (inverse of Steklov-Poincaré)

$$\mathcal{M}_{\mathcal{A}}: H^{-1/2}(\Sigma) \to H^{1/2}(\Sigma), \qquad \mathcal{M}_{\mathcal{A}}w = \mathcal{R}w|_{\Sigma}.$$

•The operator $\mathcal{M}_{\mathcal{A}}$ is continuous on $H^{1/2}(\Sigma)$ and compact, self-adjoint and positive on $L^2(\Sigma)$.

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Functional setting – cont.

We also introduce the particular solution p^* to the problem with non-homogeneous boundary conditions:

$$\begin{cases} -\Delta p^* = 0 & \text{ in } \Omega_F, \\ \frac{\partial p^*}{\partial n} = 0 & \text{ on } \Gamma_F^3 \cup \Sigma, \\ p^* = \bar{p} & \text{ on } \Gamma_F^1 \cup \Gamma_F^2 \end{cases}$$

We have that $p = p^* - \rho_f \mathcal{R} \frac{\partial^2 \eta}{\partial t^2}$. and, setting $p_{ext} = p^*|_{\Sigma}$

$$p|_{\Sigma} = p_{ext} - \rho_f \mathcal{M}_{\mathcal{A}} \frac{\partial^2 \eta}{\partial t^2}$$

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Added-mass equation

Substituting the previous expression in the structure equation we get

$$(\rho_{s}h_{s}\mathcal{I} + \rho_{f}\mathcal{M}_{\mathcal{A}})\frac{\partial^{2}\eta}{\partial t^{2}} - a\frac{\partial^{2}\eta}{\partial x^{2}} + b\eta = p_{ext} \qquad (*)$$

•Equation (*) is similar to the structure equation except for the extra term $\rho_f \mathcal{M}_A$.

•This operator represents the interaction of the fluid on the structure and acts as an extra mass (\rightarrow "added-mass" effect).

•Problem (*) admits a unique solution $\eta \in \mathcal{C}([0,\infty), H^1(\Sigma))$.



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Spectrum of the added-mass operator

- It is useful to study the behaviour of the maximum eigenvalue $\mu_{\rm max}$ of $\mathcal{M}_{\mathcal{A}}$
 - The inverse of μ_{\max} is the smallest eigenvalue of the standard Steklov-Poincaré operator.
 - μ_{max} is a purely geometric quantity.

It can be computed analytically in simple cases:

•2D fluid in rectangle: $\mu_{max} = \frac{L}{\pi \operatorname{th}\left(\frac{\pi R}{L}\right)}$. •2D axi-symmetric fluid in cylinder $\mu_{max} = \frac{L I_0\left(\frac{\pi L}{L}\right)}{\pi I_0'\left(\frac{\pi R}{L}\right)}$ where I_0 is the modified Bessel function. For R/L small, $\mu_{max} \approx \frac{2L^2}{\pi^2 R}$.

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Spectrum of the added-mass operator



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Instability of explicit algorithms

Prototype of explicit algorithm: Leap-frog for the structure and Implicit Euler for the fluid (LF-IE).

$$\begin{cases} \rho_f \frac{\mathbf{u}^n - \mathbf{u}^{n-1}}{\Delta t} + \nabla p^n = \mathbf{0} \\ \operatorname{div} \mathbf{u}^n = \mathbf{0} & \xrightarrow{\operatorname{div}} \\ \mathbf{u}^n = \frac{\eta^n - \eta^{n-1}}{\Delta t} \mathbf{n} \end{cases} \xrightarrow{div} \begin{cases} \Delta p^n = \mathbf{0} \\ \partial_n p^n = -\rho_f \frac{\eta^n - 2\eta^{n-1} + \eta^{n-2}}{\Delta t^2} \end{cases}$$

$$\rho_w h_s \frac{\eta^{n+1} - 2\eta^n + \eta^{n-1}}{\Delta t^2} + b\eta^n = p^n + p_{ext}^n \qquad \text{on } \Sigma$$

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Instability of explicit algorithms

Prototype of explicit algorithm: Leap-frog for the structure and Implicit Euler for the fluid (LF-IE).

$$\begin{cases} \rho_f \frac{\mathbf{u}^n - \mathbf{u}^{n-1}}{\Delta t} + \nabla p^n = 0\\ \operatorname{div} \mathbf{u}^n = 0 & \xrightarrow{\operatorname{div}} \\ \mathbf{u}^n = \frac{\eta^n - \eta^{n-1}}{\Delta t} \mathbf{n} \end{cases} \xrightarrow{\operatorname{div}} \begin{cases} \Delta p^n = 0\\ \partial_{\mathbf{n}} p^n = -\rho_f \frac{\eta^n - 2\eta^{n-1} + \eta^{n-2}}{\Delta t^2} \end{cases}$$

$$\rho_w h_s \frac{\eta^{n+1} - 2\eta^n + \eta^{n-1}}{\Delta t^2} + b\eta^n = p^n + p_{ext}^n \qquad \text{on } \Sigma$$

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ALE framework Partitioned algorithms Added mass effect

This algorithm is equivalent to the 3 steps difference eq.

$$\rho_w h_s \frac{\eta^{n+1} - 2\eta^n + \eta^{n-1}}{\Delta t^2} + b\eta^n = -\rho_f \mathcal{M}_{\mathcal{A}} \frac{\eta^n - 2\eta^{n-1} + \eta^{n-2}}{\Delta t^2} + p_{ext}^n$$

Proposition 1 [Causin, Gerbeau, Nobile 2004]

The explicit *Leap-Frog/Implicit Euler* algorithm is unconditionally unstable if

 $\frac{\varrho_s h_s}{\rho_f \mu_{max}} < 1$

• the scheme is unstable when $\rho_s h_s / \rho_f$ small or μ_{max} large.

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ALE framework Partitioned algorithm: Added mass effect

Sketch of the Proof. Expand η and p_{ext} on the basis of eigenvectors of $\mathcal{M}_{\mathcal{A}}$. For each component, the characteristic polynomial $\chi(s) \in \mathbb{P}^3$ of the 3 step difference equation is s.t.

$$\chi(-\infty) = -\infty, \qquad \chi(-1) = b + 4(\rho_f \mu_i - \rho_w h)/\Delta t^2$$

Hence, if $\rho_f \mu_{max} \geq \rho_s h_s$, then

 $\chi(-1) \ge 0 \qquad \Longrightarrow \qquad \exists s^* \le -1 \text{ s.t. } \chi(s^*) = 0, \qquad \forall \Delta t!!!!$



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Implicit algorithms

Prototype of implicit algorithm: Implicit Euler for the fluid and first order BDF for the structure (BDF+IE)

$$\begin{cases} \rho_f \frac{\mathbf{u}^{n+1} - \mathbf{u}^n}{\Delta t} + \nabla p^{n+1} = \mathbf{0} \\ \operatorname{div} \mathbf{u}^{n+1} = \mathbf{0} \\ \mathbf{u}^{n+1} = \frac{\eta^{n+1} - \eta^n}{\Delta t} \mathbf{n} \end{cases} \xrightarrow{\operatorname{div}} \begin{cases} \Delta p^{n+1} = \mathbf{0} \\ \partial_n p^{n+1} = -\rho_f \frac{\eta^{n+1} - 2\eta^n + \eta^{n-1}}{\Delta t^2} \end{cases}$$

$$\rho_w h_s \frac{\eta^{n+1} - 2\eta^n + \eta^{n-1}}{\Delta t^2} + b\eta^{n+1} = p^{n+1} + p_{ext}^{n+1} \qquad \text{on } \Sigma$$

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ALE framework Partitioned algorithms Added mass effect

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ALE framework Partitioned algorithm: Added mass effect

equivalent to the 2 step difference equation

$$\left(\rho_{w}h_{s}\mathcal{I}+\rho_{f}\mathcal{M}_{\mathcal{A}}\right)\frac{\eta^{n+1}-2\eta^{n}+\eta^{n-1}}{\Delta t^{2}}+b\eta^{n+1}=p_{ext}^{n+1}$$

•Stable discretization for any Δt .

•Implicit discretization \longrightarrow need subiterations. Partitioned algorithms: let's consider the two strategies

- Dirichlet/Neumann (D-N): at each iteration solve the fluid with imposed velocity at the interface and the structure with imposed loads.
- Neumann/Dirichlet (N-D): solve the fluid equations subjected to the structure load and update structure displacement.

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ALE framework Partitioned algorithm: Added mass effect

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ALE framework Partitioned algorithms Added mass effect

Dirichlet-Neumann method

ii.

given an initial guess η_0^{n+1} , we solve for each $k=1,2,\ldots$

i.
$$\Delta p_k = 0$$
 in Ω_F

$$\partial_{\mathbf{n}} p_k = -
ho_f rac{\eta_{k-1} - 2\eta^n + \eta^{n-1}}{\Delta t^2}$$
 on Σ

$$ho_w h_s rac{ ilde \eta_k - 2\eta^n + \eta^{n-1}}{\Delta t^2} + b ilde \eta_k = p_k + p_{ext}^{n+1}$$
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iii. $\eta_k = \omega \tilde{\eta}_k + (1 - \omega) \eta_{k-1}$

•equivalent to a fixed point algorithm on η^{n+1} .

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ALE framework Partitioned algorithm: Added mass effect

Proposition 2

The Dirichlet-Neumann iterative algorithm converges iff

 $0 < \omega < \frac{2 + \epsilon}{1 + \rho_f \mu_{max} / \varrho_s h_s + \epsilon}$

where
$$\epsilon = b\Delta t^2/\varrho_s h_s$$

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•In the limit $\Delta t \rightarrow 0$, whenever the explicit algorithm diverges $(\rho_f \mu_{max} > \rho_s h_s)$, the D-N iterative method needs a relaxation parameter strictly smaller than 1 to converge.

•The algorithm needs more relaxation for ρ_s/ρ_f small and μ_{max} large.

ALE framework Partitioned algorithms Added mass effect

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Mathematical problem Numerical approximation and stability analysis Absorbing boundary conditions

Added mass effect

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ALE framework Partitioned algorithms Added mass effect

Neumann-Dirichlet subiterations

given an initial guess η_0^{n+1} , we solve for each $k = 1, 2, \ldots$

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•Again, this iterative algorithm can be seen as a fixed point method on $\eta^{n+1}.$

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ALE framework Partitioned algorithms Added mass effect

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ALE framework Partitioned algorithms Added mass effect

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The N-D iterative method converges to the solution of BDF1+IE if and only if, for all i = 1, 2, ...,

$$0 < \omega < \frac{2\rho_f}{\rho_f + (\rho_s h_s + a\Delta t^2)/\mu_i}$$

•At the continuous level, $\inf_i \mu_i = 0$.

•At the discrete level, $\mu_{min} = O(h)$. Hence, the relaxation parameter needed to have convergence tends to zero with h !!



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ALE framework Partitioned algorithms Added mass effect

Back to the non linear problem - ongoing research

- Implicit coupling is needed for stability purposes. The non-linear problem can be written at each time step as an interface equation on the structure displacement and velocity
- Several techniques have been proposed to solve efficiently the coupled non-linear problem:
 - Fixed point iterations with Aitken extrapolation [S. Deparis, M. Fernandez]
 - Non linear Domain Decomposition algorithms (DN, ND, NN) [M. Discacciati, S. Deparis, A. Quarteroni]
 - $\bullet\,$ Exact Newton on the interface equation [M. Fernandez, Moubachir] $+\,$ GMRES to solve the tangent operator
 - Quasi-Newton; tangent operator approximated with the added mass model [J.F. Gerbeau, M. Vidrascu]
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Numerical results – pressure pulse in a pipe



(A. Moura, MOX)

Solved with linear 3D elasticity + exact Newton iterations + Homogeneous Neumann b.cs on the outflow section



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Numerical results - Carotid bifurcation



(A. Moura, MOX)

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Solved with linear 3D elasticity + exact Newton iterations + Homogeneous Neumann b.cs on the outflow sections



1D hyperbolic model Absorbing boundary conditions

Outline

Introduction

- 2 Mathematical problem
 - Governing equations
 - Global weak formulation
 - Energy inequality
- Oumerical approximation and stability analysis
 - ALE framework
 - Partitioned algorithms
 - Added mass effect
- Absorbing boundary conditions
 - 1D hyperbolic model
 - Absorbing boundary conditions
- 5 Numerical results

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1D hyperbolic model Absorbing boundary conditions

1D hyperbolic model

• The fluid-structure problem behaves like a propagative system

• For a cylindrical pipe, the propagative nature can be seen by integrating the equations on each transversal section.

Averaged variables

flux:

$$Q(z) = \int_{S(z)} u_z$$
Area:

$$A(Z) = |S(z)|$$
mean pressure:

$$\bar{p}(z) = \frac{1}{A(z)} \int_{S(z)} p$$

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Averaged variables

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1D hyperbolic model Absorbing boundary conditions

1D hyperbolic model

Solve for $z \in (a, b), t > 0$ $\begin{cases} \frac{\partial A}{\partial t} + \frac{\partial Q}{\partial z} = 0, \quad (\text{mass equation}) \\ \frac{\partial Q}{\partial t} + \frac{\partial}{\partial z} \left(\frac{Q^2}{A}\right) + \frac{A}{\rho} \frac{\partial \overline{p}}{\partial z} = -K_r \frac{Q}{A}, \quad (\text{momentum equation}) \\ \overline{p}(A; A_0, \beta) = \beta \frac{\sqrt{A} - \sqrt{A_0}}{A_0} \quad \text{with} \quad \beta = \frac{\sqrt{\pi} h_0 E}{1 - \nu^2} \quad (\text{algebraic law}) \end{cases}$

It is a full hyperbolic system with characteristic speeds λ_{1,2} = Q/A ± c, and c² = A/ρ ∂p/∂A (in physiological conditions λ₁ > 0 and λ₂ < 0)

• It admits the characteristic variables $W_{1,2} = \frac{Q}{A} \pm \int_{A_0}^{A} \frac{c(s)}{s} ds$



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1D hyperbolic model Absorbing boundary conditions

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• It is a full hyperbolic system with characteristic speeds $\lambda_{1,2} = \frac{Q}{A} \pm c$, and $c^2 = \frac{A}{\rho} \frac{\partial \overline{\rho}}{\partial A}$ (in physiological conditions $\lambda_1 > 0$ and $\lambda_2 < 0$)

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1D hyperbolic model Absorbing boundary conditions

Absorbing boundary condition

- The condition $W_2 = 0$ is an absorbing boundary condition for the 1D model (no information entering the domain from the right)
- Idea: apply the same condition to the 3D problem

Absorbing boundary condition

$$W_2(Q,\bar{p}) = \frac{Q}{A} - \frac{2}{\sqrt{\varrho_0^5}} \left(\sqrt{\bar{p} + \beta \sqrt{A_0}} - \sqrt{\beta \sqrt{A_0}} \right) = 0 \quad \text{on } \Gamma_{out}$$

- Use an explicit approach:
 - either impose a Neumann boundary condition σ_fⁿ⁺¹ · n = p̄ⁿ⁺¹n such that W₂(p̄ⁿ⁺¹, Qⁿ) = 0
 - or impose a outflow flux Qⁿ⁺¹ such that W₂(Qⁿ⁺¹, p̄ⁿ) by a Lagrange Multiplier

1D hyperbolic model Absorbing boundary conditions

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 - either impose a Neumann boundary condition σ_fⁿ⁺¹ · n = p̄ⁿ⁺¹n such that W₂(p̄ⁿ⁺¹, Qⁿ) = 0
 - or impose a outflow flux Qⁿ⁺¹ such that W₂(Qⁿ⁺¹, p
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1D hyperbolic model Absorbing boundary conditions

Absorbing boundary condition

- The condition $W_2 = 0$ is an absorbing boundary condition for the 1D model (no information entering the domain from the right)
- Idea: apply the same condition to the 3D problem

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Outline

Introduction

- 2 Mathematical problem
 - Governing equations
 - Global weak formulation
 - Energy inequality
- Interpretation and stability analysis
 - ALE framework
 - Partitioned algorithms
 - Added mass effect
- 4 Absorbing boundary conditions
 - 1D hyperbolic model
 - Absorbing boundary conditions

5 Numerical results

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Numerical results – pressure pulse in a pipe



- Axisymmetric formulation
- Algebraic structure law
- Inlet pressure:

$$P_{in} = \begin{cases} 5000 \frac{dyne}{cm^3} & t \le 5ms \\ 0 & t > 5ms \end{cases}$$

- mean pressure on cross section at x = 1.4 cm
- Comparison between absorbing and non-absorbing (homogeneous Neumann boundary conditions

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- A very well known analytical solution in vascular dynamics is the Womersley profile
 - Prototype of pulsatile flow
 - Feature flow reversal
- Same geometry as before but with rigid wall
- Inlet pulsatile flow rate

 $Q_{in} = \sin(2\pi t) cm^3 / sec$

• Outlet stress free cond.

(C. Vergara, MOX)

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Numerical results - Fluid-structure equivalent



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(B)

•Axial velocity profile on Γ_{out}



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- The fluid-structure solution on Γ_{out} looks delayed by ≈ 9 ms.
- We superpose in the plot the Womersley solutions delayed by 9 *ms*

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Black: Womersley profile $u_W(t)$ Red: Fluid-structure solution $u_{FS}(t)$ Blue: Delayed Womersley sol. $u_W(t - 9ms)$



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Numerical results – A more realistic case



(A. Moura, MOX)

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Solved with linear 3D elasticity $+ \; \text{exact Newton iterations} \; + \; \text{absorbing boundary conditions}$